

The Collagenase of the Bacterium *Clostridium histolyticum* in the Treatment of Irradiation-Induced Capsular Contracture

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Abstract

Background Irradiation therapy is an important pillar in the treatment of breast cancer. However, it can trigger capsular fibrosis, the most significant complication of implant-based breast reconstruction. As collagen is the main component of fibrotic capsules, the collagenase of the bacterium *Clostridium histolyticum* poses a potential treatment option for this pathological condition.

Methods Thirty-six rats received miniature silicone implants on their backs. On day 1, the implant sites of two groups were irradiated with 10 Gy. On day 120, one irradiated group received collagenase injections into the implant pockets ($n = 12$). Non-irradiated ($n = 12$) and irradiated capsules ($n = 12$) were injected with plain solvent solution serving as controls. Data were analyzed by

means of in vivo imaging, histology, immunohistochemistry and gene expression analysis.

Results Compared with both controls, the injection of collagenase led to significantly thinner capsules. This was verified by in vivo imaging and histology. Although irradiation provoked alterations in capsule collagen structure and vessel wall thickness, the application of collagenase resulted in a significant reduction of collagen density. This was accompanied by an up-regulation of VEGF-A gene expression. Of note, hematoma formation inside the implant pocket occurred in two cases after collagenase injection.

Conclusions The collagenase of the bacterium *Clostridium histolyticum* is effective in degrading irradiation-induced capsular fibrosis around silicone implants. Hematoma formation occurred most likely because of irradiation-induced alterations in vessel wall architecture and capsule vascularization. Further studies need to be performed to address the clinical safety of this novel treatment option.

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Introduction

The insertion of silicone implants for reconstructive or aesthetic purposes is one of the most frequently performed procedures in plastic surgery [1]. The most prevalent complication after this procedure is the formation of capsular contracture [2–4]. Its incidence rate is heavily influenced by factors like site of implant placement, follow-up period, implant surface and especially indication for implant insertion [5–9]. Interestingly, capsular contracture

occurs three times more frequent in patients who received an implant for breast reconstruction after breast cancer treatment compared with aesthetic indications [10]. Nevertheless, approximately 70% of women undergoing reconstruction after mastectomy decide on silicone implants, and of those, up to 50% develop capsular contracture [11–13]. To date, revision surgery is the only viable treatment option for clinically relevant capsular contracture [14–16].

As the fibrotic capsule mainly consists of collagen, the collagenase of the bacterium *Clostridium histolyticum* (CCH) might be a viable treatment option for capsular contracture. This drug is already FDA-approved for the treatment of Dupuytren's contracture, as well as Peyronie's and Ledderhose diseases [17–19].

In our previous studies, CCH injections led to a dose-dependent reduction of fibrotic capsules around silicone implants [20, 21]. Despite these encouraging results, translation of this therapy to clinical application poses a barrier. Post-mastectomy irradiation can lead to significant alterations in morphology, thickness and collagen organization of the fibrotic capsules, which could potentially influence the effectiveness and safety of CCH application [22].

The aim of this study was to investigate the effect of CCH on irradiation-induced capsular contracture tissue in a standardized rat model. The primary endpoint of this study was the effect of CCH on capsule thickness and density after irradiation. Analyses of gene expression and immunohistochemistry were considered secondary endpoints.

Methods

Study Design

Sample size calculation was based on our previous studies [20, 23]. With the assumption of equal standard deviations, type I error < 0.05, type II error < 0.2 and effect size of 1.1, the number of animals needed is 12 per group. Therefore, we included 36 rats in this study, divided into three groups (CG[Øirrad], CG[irrad] and CCH[irrad]). All animals received silicone implants in a sub-muscular pocket on their backs on day 0. On day 1, rats of groups CG[irrad] and CCH[irrad] received irradiation with 10 Gray (Gy). After stable capsule formation on day 120, a collagenase solution of 0.3 mg/ml (CCH[irrad]) or 0.0 mg/ml CCH (CG[Øirrad] and CG[irrad]) was injected into the implant pockets. On day 130, animals underwent MR imaging and were euthanized and subsequent analyses were performed as described below. According to a study by Sengupta et al. [24], 1 month of an adult rat's life

equates to 3 human years. Therefore, the follow-up period of this manuscript equates to one human year.

Animal Model

The research protocol was approved by the Harvard Medical Standing Committee on Animals (AEP No.: 05086). Female Lewis rats received miniature silicone implants with textured surfaces (Polytech Health and Aesthetic, Dieburg, Germany). Implants were inserted in a sub-muscular pocket through a 4-cm incision on the back of each rat [23]. Ten days after CCH injections, animals were euthanized and silicone implants with surrounding capsules were explanted en bloc.

Irradiation

One day after insertion of silicone implants, study groups CG[irrad] and CCH[irrad] received a single irradiation treatment at the implant site with 10 Gy. This is based on a protocol by Katzel et al. [22] in which, except for the increase in fibrotic tissue, no other harmful side effects of the irradiation are reported. Irradiation was administered using a Mark I 68A irradiator (JL Shepherd and Associates, San Fernando, CA) with a Cesium 137 irradiation source.

Collagenase Injection

We used the collagenase of the bacterium *Clostridium histolyticum* (CCH, Xiaflex, Endo Pharmaceuticals, Malvern, USA). CCH (0.1 ml) was injected at a concentration of either 0.0 mg/ml (CG[Øirrad] and CG[irrad]) or 0.3 mg/ml (CCH[irrad]) 120 days after surgery, based on previously established protocols [20, 23]. Solutions were injected through a small incision on top of the implant between capsule and implant shell with a blunt needle.

Clinical Evaluation

Daily after injections, all animals were monitored for the occurrence of systemic and local side effects like skin perforation or hematoma formation.

Magnetic Resonance Imaging

Animals underwent magnetic resonance imaging (MRI) on day 130 based on previously established protocols [9, 20, 23]. We used an ultra-high-field MRI preclinical scanner, 7.0T Bruker BioSpec[®] (Billerica, MA). Imaging parameters were set as previously described [20, 23]. Data were analyzed via ImageJ (v. 1.46, NIH, USA) and 3D Volume measurement plug-in "VOLUMEST" [25]. Capsule thickness was measured in three planes from the outer

margin of the implant to the outer side of the skin (Fig. 1). Capsule volume was measured as previously described using “VOLUMEST” plug-in for ImageJ [9]. Results are expressed as mean \pm standard deviation (SD).

Histology

After fixation in formaldehyde, capsule specimens were subsequently embedded in paraffin for histologic analysis.

Capsule thickness was assessed by two blinded investigators using Masson trichrome staining. Thickness of fibrotic capsules was measured at the thickest part of the capsule between the surface of the implant and the first tissue that did not belong to the capsule (fat, muscle) [20, 23]. Collagen fiber density was quantified and depicted by Picosirius red staining. Under circularly polarized light, collagen thick, thin and total fiber density was quantified by counting of stained pixels with ImageJ and evaluation as the percentage of the whole image pixel count. Measurements were taken at 10 randomly chosen sites.

Additionally, wall thickness and diameter of intracapsular vessels were assessed on hematoxylin & eosin-stained slides. Measurements were taken at 20 randomly chosen vessels at a 400 \times magnification. A ratio of wall thickness to vessel diameter was formed to ensure comparability between groups. All results are given as mean \pm standard deviation.

Immunohistochemistry

Immunohistochemistry was performed using antibodies against collagen subtypes I–IV and TGF β 1 (Abcam, Cambridge, UK) as recommended by the manufacturer. After heat-mediated antigen retrieval, slides were incubated with primary and secondary antibodies. Diaminobenzidine was used for visualization, and cell nuclei were counterstained with hematoxylin. For each sample, three randomly chosen sites of the capsule were digitalized at a 20 \times magnification. Antigen density was measured as described by Schon et al. [26]. Densities are calculated as percentage of brown-colored pixels in relation to the whole image pixel count.

Quantitative Real-Time PCR

Total cellular RNA was extracted using the RNeasy Mini Kit (Qiagen, USA) and transcribed with the ABI PRISM TaqMan reverse transcription method (Applied Biosystems, USA). Table 1 shows a list of all analyzed markers with corresponding article numbers. Quantitation of gene expression was determined by means of the ABI PRISM 7900HT System (Applied Biosystems, USA). To normalize relative gene expression to expression levels of the housekeeping gene β 2-microglobulin, we applied the comparative CT ($\Delta\Delta$ CT) method. Results of expression analysis are given in relative quantitation (RQ).

Fig. 1 MRI analysis of in vivo capsule thickness. Top left: 3D-reconstruction, top right: axial plane, bottom left: sagittal plane, bottom right: coronal plane. Red lines indicate capsule thickness measurements. Scale was set by measuring the inner circle which has a diameter of 0.8 cm

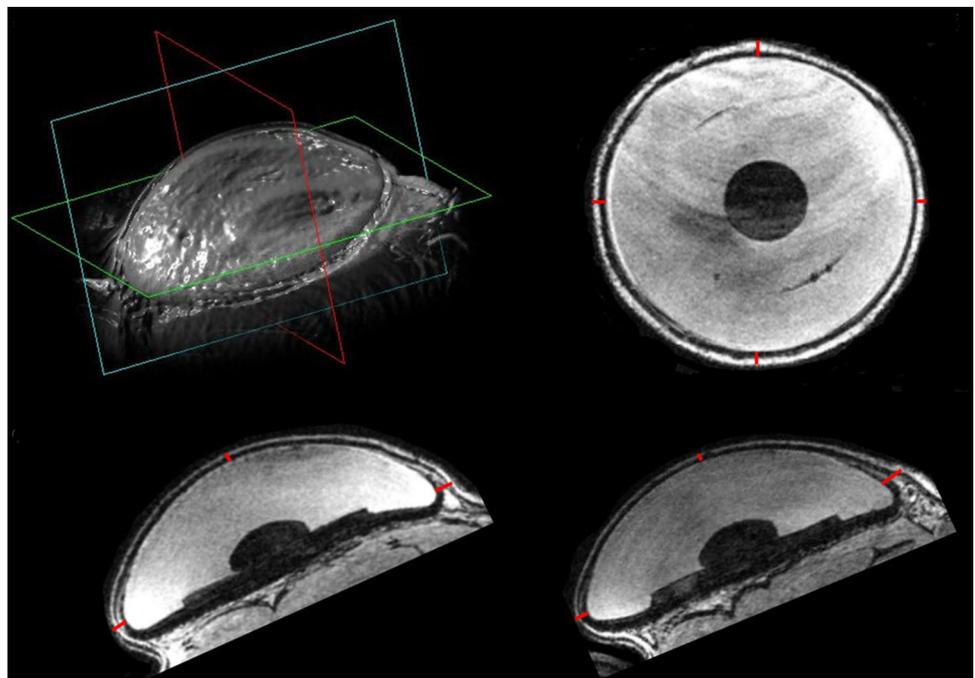


Table 1 Primers used for qRT-PCR analysis according to catalog numbers

Primer name	Catalog number
Col1a1	Rn01463848_m1
Col2a1	Rn01533081_m1
Col3a1	Rn01437660_g1
Col4a1	Rn01482927_m1
TGFβ1	Rn00572010_m1
TGFβ3	Rn01517871_m1
CD68	Rn01495634_g1
IL12	Rn01456866_m1
B2m (housekeeping gene)	Rn00560865_m1

Statistical Analysis

Statistical evaluation was performed using the Statistical Package for Social Science SPSS, Version 18.0 (SPSS Inc., Chicago, USA). Data of all groups were assessed using analysis of variance (ANOVA). Post hoc testing was performed by means of *t* test with Bonferroni correction. Results are reported as means ± standard deviations. According to Bonferroni corrections, the statistical significance level was set as $p < 0.017$.

Results

Clinical Evaluation

In two cases of group CCH[irrad], intracapsular hematoma formation occurred one day after collagenase injections (17%). Additionally, rupture of the silicone implant was observed in one animal of group CG[irrad] (8%). We did not detect any signs of skin perforation or skin laceration, implant site infection or other adverse effects.

Magnetic Resonance Imaging

Irradiated capsules of group CG[irrad] appeared to be thicker compared to CG[Øirrad]. However, differences were not statistically significant. Radiologic capsule thickness was considerably lower in group CCH[irrad] after irradiation and CCH injection when compared to both control groups, respectively (1.28 ± 0.25 vs 1.94 ± 0.23 (CG[irrad]) or 1.82 ± 0.42 mm (CG[Øirrad])). Compared to CG[irrad], differences reached statistical significance ($p < 0.017$). Results of in vivo capsule thickness measurements are depicted in Fig. 2.

In terms of capsule volume analysis, we observed a similar data distribution, yet without statistically significant differences (data not shown).

Histologic Capsule Thickness

Results of histologic capsule thickness measurements are shown in Fig. 2. Within control groups, capsule thickness was notably higher after irradiation of the implant site (CG[Øirrad] vs CG[irrad]), yet no statistical significance was detectable. In comparison with both controls, treatment with CCH was able to significantly decrease histologic capsule thickness to mean values of $144.72 \pm 30.97 \mu\text{m}$ ($p < 0.017$).

Capsule Collagen Density

The total collagen fiber density was 24.07 ± 10.02 , 35.83 ± 11.01 and $13.23 \pm 5.8\%$ for the groups CG[Øirrad], CG[irrad] and CCH[irrad], respectively. Irradiation (CG[irrad]) leads to remarkably denser fibrotic capsules when compared to CG[Øirrad]. In terms of CCH injections, we observed a considerable decrease in capsule collagen content which reached statistical significance when compared to CG[irrad].

Correlating with the results for total collagen, thick and thin fiber density was highest after irradiation of implant sites (CG[irrad]). However, statistically significant differences were not detected in the analysis of thin fiber density. For thick-fiber density, we observed the lowest values after injection of CCH which amounted to $2.74 \pm 3.06\%$. This was significantly less than in the control group CG[irrad], $p < 0.017$. Results for collagen density measurements are shown in Fig. 3.

Vessel Wall Thickness/Diameter Ratio

Figure 4 depicts the results of histologic vessel analysis. Injections of CCH (CCH[irrad]) did not lead to any alterations of vessel walls when compared to CG[irrad]. In group CG[Øirrad], we measured a mean thickness/diameter ratio of 0.46 ± 0.28 . This was significantly higher than found for both irradiated groups CG[irrad] and CCH[irrad] ($p < 0.017$).

Immunohistochemistry

Antibody staining for collagens I–IV revealed that the CCH leads to a reduction in mainly collagens I and III, whereas it omits collagen IV, as expected from the collagenase properties (data not shown). However, no statistically significant differences between groups could be identified.

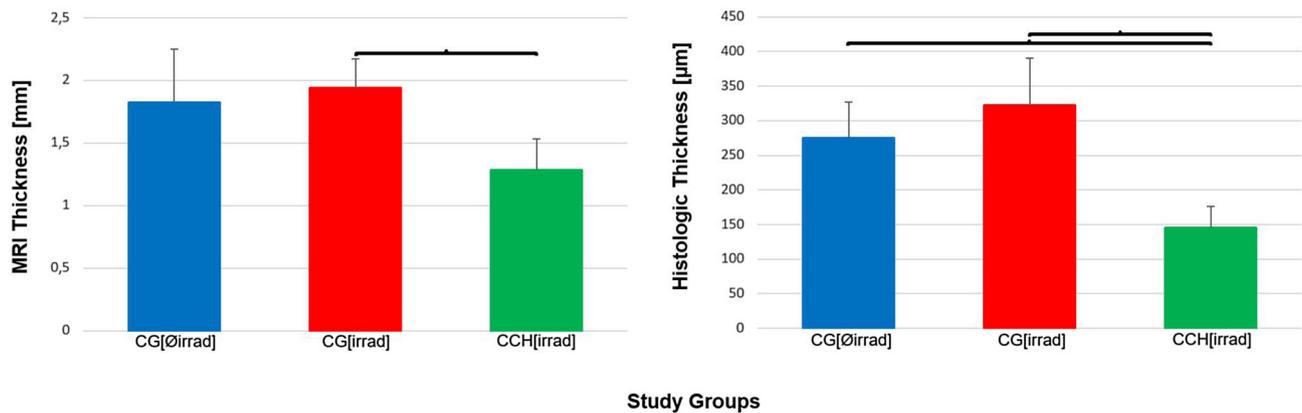


Fig. 2 MRI and histologic capsule thickness measurements. Mean values (bars) with corresponding standard deviations. Brackets indicate statistically significant differences ($p < 0.017$)

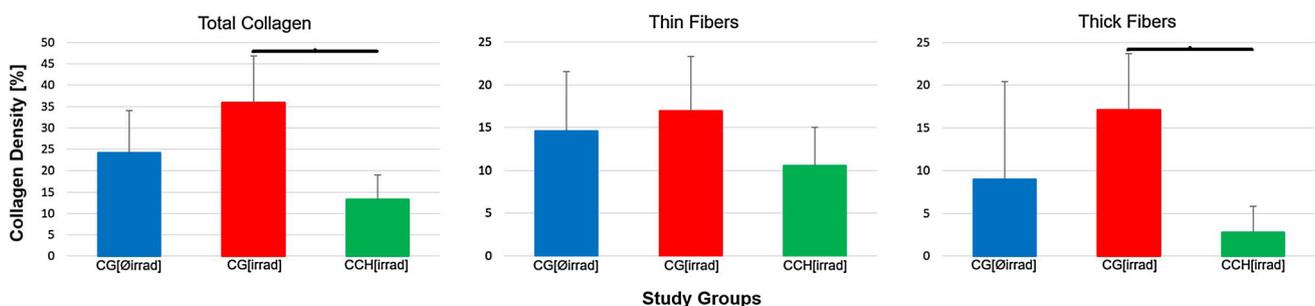


Fig. 3 Capsule collagen density measurements. Left) total collagen, middle) thin fibers, right) thick fibers. Results are given as mean values (bars) with corresponding standard deviation. Brackets indicate statistically significant differences ($p < 0.017$)

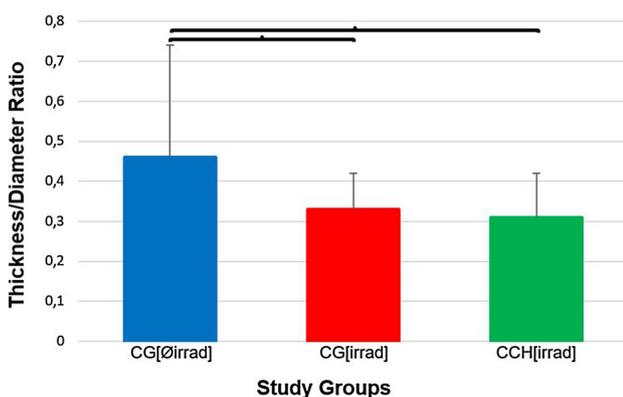


Fig. 4 Results of vessel wall analysis. Mean values (bars) with corresponding standard deviation. Brackets indicate statistically significant differences ($p < 0.017$)

qRT-PCR

A significant overexpression of CD68 was observed in CCH[irrad] compared to CG[Øirrad] ($p < 0.017$; Fig. 5). Although the expression of the profibrotic gene TGF β 1 showed higher levels after irradiation with or without CCH injections, TGF β 3 was under-expressed compared to CG[Øirrad]. However, differences were not statistically

significant. With respect to the proangiogenic marker VEGF-A, significant differences were observed between CCH[irrad] and CG[Øirrad] (RQ 5.33 ± 0.14 , $p < 0.017$) and between CCH[irrad] and CG[irrad] (RQ 5.33 ± 0.14 vs 1.96 ± 0.27 , $p < 0.017$). Significant differences for collagen subtypes I–IV and the inflammatory marker IL-12 have not been detected.

Discussion

This study demonstrates that the CCH is effective in reducing irradiation-induced fibrotic capsules surrounding silicone implants. This was determined by means of in vivo MR imaging, as well as histology. Interestingly, the combination of singular irradiation of implant sites and injection of CCH leads to a down-regulatory trend of TGF β 3 expression, whereas other inflammatory and profibrotic markers displayed a tendency toward higher expression levels. Despite these encouraging results, hematoma formation occurred in 17% of our experimental group.

Depending on tumor size, tumor entity, lymph node metastasis and resection status, radiotherapy is a crucial part of breast cancer treatment. This has to be taken into

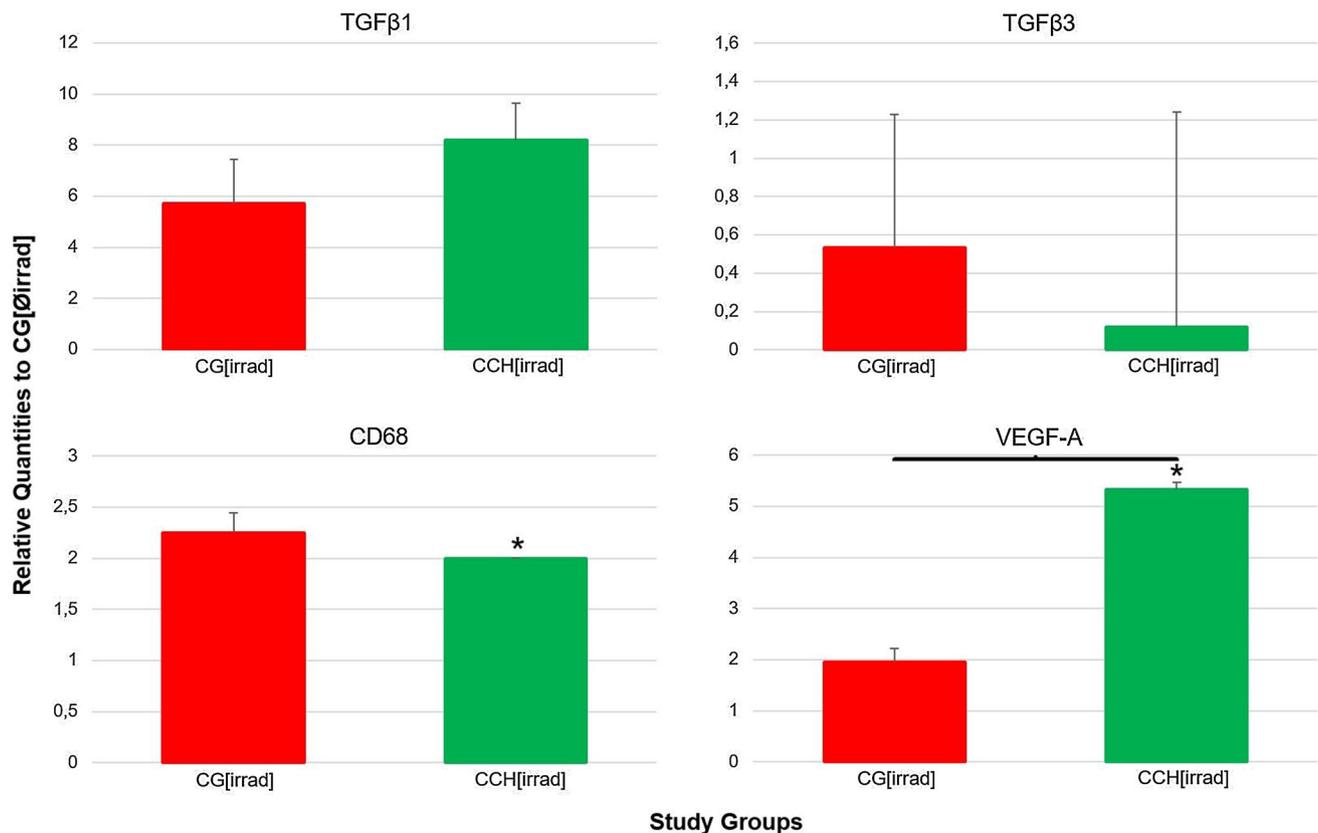


Fig. 5 Results of qRT-PCR analysis. Mean values (bars) with corresponding standard deviation. Asterisks denote statistically significant differences ($p < 0.017$) compared to CG[Øirrad]. Brackets indicate statistically significant differences between groups CCH[irrad] and CG[irrad]

account, especially when considering that approximately 70% of women undergoing reconstruction after mastectomy decide on silicone implants and 50% of those develop capsular contracture [11]. This might be most likely associated with radiation therapy. In a long-term cohort study, Cordeiro et al. [13] evaluated 1415 patients receiving silicone breast implants and demonstrated that incidence rates of capsular contracture were significantly higher in irradiated breasts. Interestingly, radiotherapy does not only affect the occurrence of capsular contracture but also the structure of the fibrotic capsule. Katzel et al. [22] investigated the impact of radiotherapy on capsular contracture formation in a mouse model. The authors detected that capsule tissue was much thicker and disorganized after irradiation. Accordingly, in our study, histologic capsule thickness was higher in the irradiated control group compared to no radiotherapy. This was apparent in MR imaging and histologic analysis. Additionally, we observed changes in collagen structure, such as denser arrangement of collagen fibers. This was accompanied by an overexpression of profibrotic and inflammatory genes like CD68 or TGFβ1.

Besides examining the effectiveness of CCH injections, several authors particularly investigated the safety of CCH

in the treatment of Dupuytren's contracture and Peyronie's disease [17, 27–29]. In a structured literature review of 59 clinical studies involving 8809 patients, Peimer et al. [27] compared the safety profile of CCH application with surgical fasciectomy. Although incidence rates for adverse effects like chronic regional pain syndrome or scar hypertrophy were noticeably lower following enzyme treatment, injury of the skin occurred in 16.2% compared to 2.8% after surgery. These skin injuries included less severe side effects like skin discoloration and blistering as well as skin exfoliation and laceration. However, skin damage did not necessitate further special medical treatment. This ties in with reports by Warwick et al. [29] who state that skin injury rates were 13% after CCH injections and that skin tears healed within 21 days without impairment of skin quality. In our previous study, we observed skin injury following collagenase treatment in 17% of cases [20]. Yet, skin tearing occurred more than 48 h after enzyme injection, a timepoint when the collagenase is expected to be inactivated already [30]. Thus, we hypothesized that the cause of skin perforation might be irritation through direct contact between the textured silicone implants and the skin after capsule digestion. This hypothesis is supported by the absence of skin perforation

after incubation of rat and human skin with six times higher CCH concentrations in our *in vitro* studies [20, 21].

In the present study, the combination of acute irradiation with CCH application led to hematoma formation within the implant pocket in 17%. In this context, Levine et al. [17] investigated the efficacy and safety of collagenase injections in patients with Peyronie's disease. In this phase III study, 347 patients received multiple CCH injections (0.58 mg/ml) into Peyronie's plaques. Although Levine reported overall good clinical outcomes, hematoma formation developed in two cases. Both hematomas were treated conventionally and resolved spontaneously. Of note, both patients received further CCH injections afterward with no re-emerging side effects. In our study, hematoma formation occurred inside the implant pocket in two animals. The development of hematoma despite a low collagenase concentration might be due to irradiation of the implant site. By the induction of endothelial cell necrosis and degenerative changes, irradiation therapy can cause inflammation of vessels [31]. Concurrent, irradiation affects and reduces the oxygen supply of the targeted tissue and thus leads to hypoxia, the most important trigger of proangiogenic factor release [32]. These aspects are reflected by the statistically significant overexpression of VEGF-A in the presented study. VEGF-A is a proangiogenic factor found in almost all vascularized tissues [33]. It is considered a key player in the induction of new vessel formation through angiogenesis and vasculogenesis as well as the increase in vessel permeability [33–35]. In addition to these irradiation-induced changes, several studies described a growth of vessel wall thickness through hyperplasia after radiotherapy [36–38]. Interestingly, an experimental dog model by Powers et al. [39] demonstrated that fractionated radiation results in vascular wall hyperplasia, whereas acute radiotherapy inhibited vascular wall thickening. This is consistent with our observations. We measured a significantly lower vessel wall thickness/diameter ratio after both, irradiation alone and in combination with CCH application. We hypothesize that the combination of thinner vessel walls increased angiogenesis and thus more immature blood vessels, and inflammation might lead to an increased vulnerability of blood vessels and causes hematoma formation after CCH injections. This theory is supported by the fact that we did not observe hematoma formation in our two previous *in vivo* experiments, despite the application of three times higher collagenase concentrations [20, 23].

There are several limitations to our study. For breast reconstruction or augmentation, two different kinds of silicone implants with smooth or textured surfaces are commonly used in clinical practice. Although the influence of implant surface could not yet be fully investigated, a recent meta-analysis by Liu et al. [40] linked smooth

implants to increased rates of capsular contracture. In our study, we only inserted implants with textured surfaces. Therefore, the results presented in this study do not allow conclusions on the influence of different silicone implants on the effectiveness of CCH injections. Additionally, implants were placed under the panniculus carnosus muscle which, compared to the implant coverage with the pectoralis muscle in a clinical setting, poses a much thinner muscle layer.

Capsular contracture is defined by clinical symptoms like hardness, breast deformity or pain. Yet, primary endpoints of this study were radiologic and histologic assessments of the capsule tissue. This is due to the difficult evaluation of corresponding clinical symptoms in animal models. It could be argued that the data acquired in our study do not reflect improvement of symptoms. However, several studies demonstrated a significant correlation between capsule thickness and collagen density with clinical symptoms and Baker's grade [41–43]. Therefore, reductions of these parameters can indirectly suggest clinical improvement.

Furthermore, our model used single-time irradiation to induce capsular fibrosis around the implant. Clinical protocols for breast cancer therapy, however, apply multiple, fractionated irradiation doses which allow for the application of higher total doses while reducing side effects. Thus, our study does not allow conclusions to what extent different irradiation regimen influence capsule formation, capsule quality and effectiveness of CCH injections. The above-mentioned aspects warrant further experimental analyses before proceeding to clinical trials. Furthermore, if this novel treatment is proven effective, a cost-effect study compared to the current gold-standard, namely capsulectomy with implant exchange, should be performed in the future.

Conclusion

CCH was capable of actively degrading irradiation-induced capsular fibrosis tissue. This novel method poses a viable non-surgical treatment option for the therapy of capsular fibrosis around silicone implants. Despite the overall encouraging results reported in this study, safety issues like hematoma formation and the potential of tumor recurrence that need to be accounted for prior to clinical testing still exist.

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Compliance with Ethical Standards

Conflict of interest The authors declare that they have no conflict of interest.

Ethical Approval All applicable institutional and national guidelines for care and use of animals were followed (AEP No.: 05086).

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