



Quantification of Liver Fat in NAFLD: Available Modalities and Clinical Significance

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Abstract

Purpose of Review To review the available modalities for quantification of liver fat in nonalcoholic fatty liver disease (NAFLD) and their clinical significance.

Recent Findings Ultrasonography remains the first line imaging used to diagnose NAFLD as it is widely available and relatively inexpensive. Controlled attenuation parameter can be used as a screening tool for fatty liver as it is reasonably accurate and provides simultaneous estimation of hepatic fibrosis. Magnetic resonance imaging proton density fat fraction and magnetic resonance spectroscopy are the most accurate noninvasive modalities for quantification of hepatic steatosis. Liver biopsy remains the gold standard but is limited by the invasive nature of the procedure, and observer and sampling variability. This may be improved with novel computer-assisted stereological analysis or second harmonic generation microscopy.

Summary Understanding the advantages and disadvantages of each of the modalities will help one choose the most suitable method for quantifying hepatic steatosis in NAFLD.

Keywords Hepatic steatosis · MRI-PDF · MRS · CAP

Introduction

Nonalcoholic fatty liver disease (NAFLD) has become the leading cause of chronic liver disease in the world [1]. The global prevalence of NAFLD has been reported to be 25% based on a meta-analysis [2]. NAFLD is closely associated with obesity and is considered the liver manifestation of the metabolic syndrome. Patients with NAFLD have an increased mortality rate when compared with the general population, mainly due to cardiovascular disease [3, 4]. Identifying patients with NAFLD represents an important first step towards providing more focused lifestyle advice to ameliorate the disease as well as further assessment for other components of the metabolic syndrome, which should be addressed accordingly, if present [5]. The ability to quantify liver fat allows monitoring over time, which is important for evaluation of lifestyle

intervention or medical therapy, in both clinical trial and real-world settings. This paper aimed to review the currently available modalities for quantifying liver fat in NAFLD and their clinical significance.

Ultrasonography

Ultrasonography (US) for assessment of hepatic steatosis is commonly qualitative in nature and typically consists of visual assessment of hepatic echogenicity compared with kidney cortex echogenicity, evaluation of echo penetration into the deep portion of the liver, and determination of the clarity of blood vessel structures in the liver. Normal liver echogenicity is graded as grade 0, while slight increase in liver echogenicity is considered mild steatosis (grade 1). Slight impairment in visualization of intrahepatic vessels and diaphragm with increase liver echogenicity is categorized as moderate steatosis (grade 2). In severe steatosis (grade 3), hepatic echogenicity is markedly increased, in addition to poor penetration to the posterior segment of the right lobe of the liver and poor visualization of hepatic vessels and diaphragm [6, 7]. A previous meta-analysis reported that US is reliable and accurate in detecting moderate-to-severe fatty liver with sensitivity of

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84.8% and specificity of 93.6% [8•]. However, US has several limitations, including being highly operator-dependent [9], has poor accuracy in diagnosing mild steatosis [7], and may be less accurate to diagnose steatosis in patients with underlying hepatic fibrosis [10]. A recent study revealed that the sensitivity of US was only 65.1% when compared with magnetic resonance imaging proton density fat fraction (MRI-PDFF) in diagnosing mild steatosis [11]. To improve the accuracy, computer-assisted quantitative US techniques have been developed for the assessment of hepatic steatosis [12]. The most widely reported technique is the computerized hepatorenal index with two studies showing sensitivities and specificities of more than 90% in diagnosing hepatic steatosis of $\geq 5\%$ [13•, 14]. In this technique, the ratio between the echogenicity of the liver and kidney cortex is calculated and analyzed using a histogram. However, a more recent study suggested that the hepatorenal ratio was not as good, while acoustic structure quantification (ASQ) from ultrasound echo amplitude was better for the assessment of hepatic steatosis. By using magnetic resonance spectroscopy (MRS) as the reference standard, the area under receiver operating characteristic curve (AUROC) of using the ASQ for diagnosing hepatic steatosis $\geq 10\%$ was 0.959, with sensitivity of 86.2% and specificity of 100%, while the AUROC of using hepatorenal ratio was only 0.772, with sensitivity of 72.4% and specificity of 73.3% [15, 16]. Another quantitative US technique that measures backscatter coefficient was demonstrated to be accurate in quantifying hepatic steatosis $\geq 5\%$ using the MRI-PDFF as the reference. The sensitivity and specificity were reported as 87–93% and 91–97%, respectively [17]. Overall, US remains the first-line imaging used to diagnose NAFLD as it is noninvasive, widely available, and relatively inexpensive.

Computed Tomography

Hepatic steatosis evaluation by computed tomography (CT) scan is based on the measurement of attenuation value of liver parenchyma, using Hounsfield units (HUs). Different tissue composition will have different attenuation value in HUs, for example, it is usually -100 HU for fat and around 30–40 HU for soft tissue. With hepatic steatosis, the attenuation value of the liver parenchyma is reduced [12]. Absolute liver attenuation value is developed as a quantitative method to measure steatosis [18]. This is generally performed using unenhanced CT scan to avoid the potential changes in attenuation after contrast injection despite some studies reporting similar efficacy with contrast-enhanced CT. However, the accuracy of the absolute attenuation value for the quantification of hepatic steatosis may be limited by intra- and inter-scanner variability [19]. Established quantitative CT techniques of measuring liver-to-spleen attenuation ratio (CT L/S) and liver-to-spleen difference in attenuation (CT L-S) are able to

limit the variability. In these techniques, the spleen, which generally has a lower attenuation value, is used as an internal control. CT has been reported to be reasonably accurate in diagnosing moderate to severe steatosis but lack the sensitivity to detect mild steatosis [18, 20]. The sensitivity of CT in detecting hepatic steatosis $\geq 5\%$ has been reported to be 50.5 to 67.7% using the MRI-PDFF as reference standard [21]. More importantly, the ionizing radiation from CT deters clinician in using it as a routine tool for quantification of hepatic steatosis. The assessment of hepatic steatosis by CT is usually limited to patients who have undergone CT scan for other reasons or to potential liver donor who will need a CT scan of the liver for pre-operative assessment.

Magnetic Resonance Imaging

Evaluation of fat with magnetic resonance imaging (MRI) is common by chemical-shift imaging (CSI) principal, where MRI detect different resonance frequencies between protons bound to water and fat. In a regular MRI sequence, images in “in-phase (IP)” and “opposed phase (OP)” are produced at specific echo times when water and fat signals are added and subtracted. This can produce a qualitative or semi-quantitative assessment of hepatic steatosis. In the presence of fatty liver, the liver will appear dark in opposed phase due to signal loss. Subsequently, dual-echo CSI was developed for fat quantification based on a pair of OP and IP images, but there were biased from T1- and T2*-relaxation effects. To improve accuracy, T1-independent, T2*-corrected proton density fat fraction (PDFF) methods were developed based on multiple-echo CSI that acquire three or more consecutive pairs of OP and IP echoes. Meanwhile, spectral fat modeling was developed to be applied in the T1-independent, T2*-corrected multi-echo CSI technique for more precise fat quantification. This MRI-PDFF technique analyses vector sum of all signals from fat and water of the entire liver and is able to avoid sampling error [10, 12, 22, 23]. This method can assess the fat content of the entire liver in a short breath-hold, in about 20 s. The MRI-PDFF technique has high accuracy in evaluating liver steatosis. The AUROC for diagnosing hepatic steatosis $\geq 5\%$ with histology as reference standard has been reported to be 0.98 in a recent meta-analysis [24].

Meanwhile, the MRS directly measures the chemical composition within tissue, usually based on the acquisition of data from a single voxel (typically $2\text{ cm} \times 2\text{ cm} \times 2\text{ cm}$ to $3\text{ cm} \times 3\text{ cm} \times 3\text{ cm}$ in size). Spectral tracing of fat and water peaks are attained from the MRS, then PDFF is calculated by signal intensities derived from protons bound to fat divided by amount from all protons in the liver, specifically those bound to fat and water. Despite MRS being regarded as the gold standard MRI technique for hepatic fat quantification, this technique may be limited by sampling error, similar to liver biopsy, especially in

cases with irregular hepatic fat distribution [10, 12, 22, 23]. The MRS is also time-consuming and requires technical expertise for its acquisition and analysis. A summary of meta-analyses on the MRI and MRS for the quantification of hepatic steatosis can be found in Table 1 [24, 25••, 26, 27].

The MRI and MRS have consistently outperformed CT or US in diagnosing and grading of hepatic steatosis [6, 7]. A meta-analysis reported the mean sensitivity and specificity of MRI (82.0–97.4% and 76.1–95.3%) and MRS (72.7–88.5% and 92.0–95.7%) compared with US (73.3–90.5% and 88.1–94.6%) and CT (46.1–72.0% and 76.1–95.3%) for the diagnosis of hepatic steatosis [25••]. On the other hand, the MRI-PDF and MRS were reported to be similar in accuracy in quantification of hepatic steatosis, when compared with liver histology in NAFLD patients, including in mild hepatic steatosis [28–30]. These techniques were reliable and highly reproducible [31, 32]. There have been studies suggesting that the MRS and MRI-PDF could serve as a better reference standard to quantify hepatic steatosis compared with current gold standard of liver biopsy. At the moment, the MRI-PDF has been validated as a modality to be used for early-phase clinical trials to assess hepatic steatosis [33–35]. In addition, to comprehensively evaluate the liver, it is feasible to assess fibrosis by colocalization of MRI-PDF-derived fat maps and MR elastography-derived stiffness maps at the same settings [36], besides the ability to add a standard liver MRI protocol to assess for structural abnormalities of the liver, if indicated. In a longitudinal study, the MRI-PDF and MRS correlated well and the MRI-PDF was more sensitive than histology in

detecting small increases or decreases in the liver fat content [37••]. A relative reduction of about 30% in liver fat based on the MRI-PDF was associated with 2 points or more reduction in nonalcoholic fatty liver disease (NAFLD) activity score (NAS) and had been suggested as a marker for significant improvement in clinical trials [38].

The disadvantage of using the MRI-PDF or MRS is that the presence of hepatic fibrosis may reduce the correlation with hepatic steatosis [28]. Moreover, MRS has limited clinical applicability as not every MRI scanner is equipped with MRS capabilities and sophisticated post-processing methods are required for MRS. On the other hand, the MRI-PDF can be used on any clinical MRI platform and is therefore more widely available. Moreover, it allows mapping of fat of the entire liver while MRS measures fat in only a small region of interest [39]. Overall, the high cost and limited availability of MRI scanner limit its use for quantification of hepatic steatosis in day-to-day clinical practice.

Controlled Attenuation Parameter

Controlled attenuation parameter (CAP) is the decrease in amplitude of ultrasound propagating through liver tissue that can be estimated using the same radiofrequency data used for estimation of liver stiffness using Fibroscan (Echosens, France, Paris), an ultrasound-based vibration-controlled transient elastography device [1, 40•]. CAP has been shown to correlate well with hepatic steatosis in several initial studies

Table 1 Summary of meta-analyses on MRI for quantification of hepatic steatosis

Author (year)	Number of studies and patients	MRI technique	Reference standard	Results
Gu J et al. 2019 [27]	6 studies 635 patients	MRI-PDF	Histology	Diagnosis of steatosis grade \geq S1: AUROC 0.98, sensitivity 0.93, specificity 0.94 Diagnosis of steatosis grade \geq S2: AUROC 0.91, sensitivity 0.74, specificity 0.90 Diagnosis of steatosis grade \geq S3: AUROC 0.90, sensitivity 0.74, specificity 0.87
Qu Y et al. 2019 [24]	13 studies 1100 patients	MRI-PDF	Histology	Diagnosis of steatosis grade \geq S1: AUROC 0.98 Diagnosis of steatosis grade \geq S2: AUROC 0.91, sensitivity 0.83, specificity 0.89 Diagnosis of steatosis grade \geq S3: AUROC 0.92, sensitivity 0.79, specificity 0.89
Zheng D et al. 2017 [26]	8 studies 934 living liver donors	MRI and/or MRS	Histology	For detection of hepatic steatosis: AUROC 0.92, sensitivity 0.89, specificity 0.84 For detection of substantial hepatic steatosis (> 10 to > 30%): AUROC 0.96, sensitivity 0.91, specificity 0.89
Bohte et al. 2011 [25••]	46 studies 4715 patients	MRI or MRS	Histology	MRI for detection of hepatic steatosis: sensitivity 82.0–97.4%, specificity 76.1–95.3% MRS for detection of hepatic steatosis: sensitivity 72.7–88.5%, specificity 92.0–95.7%

that consisted of patients with chronic liver disease of various aetiologies [41•, 42–46]. A subsequent study on 101 NAFLD patients and 60 non-NAFLD controls found that it was excellent for the diagnosis of significant hepatic steatosis, but its accuracy was impaired by increased body mass index and it was less accurate to distinguish between the different grades of significant hepatic steatosis. In the overall population, the AUROC of CAP for diagnosis of steatosis grade \geq S1, \geq S2, and S3 was 0.97, 0.86, and 0.75, respectively. Among non-obese patients, the AUROC for diagnosis of steatosis grade \geq S1 and \geq S2 was 0.99 and 0.99, respectively. However, among obese patients, the AUROC for diagnosis of steatosis grade \geq S1, \geq S2, and S3 was 0.92, 0.64, and 0.58, respectively. The lower diagnostic accuracy of CAP in obese patients was thought to be due to the thicker subcutaneous tissue in these patients [47•]. This was confirmed by a subsequent study that found the diagnostic accuracy of CAP to be lower in patients with skin capsular distance (SCD) $>$ 25 mm compared with patients with SCD $<$ 25 mm [48•]. In general, studies with larger proportion of NAFLD patients, greater body mass index, and higher grades of hepatic steatosis tended to produce less satisfactory diagnostic accuracy [40•, 41•, 42–46, 47•, 48•, 49–57]. A summary of the studies from which this observation was based on can be found elsewhere [58•]. Subsequent studies that evaluated CAP for the diagnosis of steatosis grades using liver biopsy as reference standard are summarized in Table 2 and a similar trend was observed [58•, 59–63, 64•, 65, 66, 67•, 68–75].

An individual patient data meta-analysis that included 2735 patients with chronic liver disease of various aetiologies defined the cutoffs for CAP for the diagnosis of steatosis grades \geq S1, \geq S2, and S3, which were 248 dB/m, 268 dB/m, and 280 dB/m, respectively. However, adjustments were recommended for several factors which were found to impact on CAP. These included deducting 10 dB/m from the CAP value for NAFLD patients, deducting 10 dB/m for patients with diabetes mellitus, and deducting or adding 4.4 dB/m for each unit of BMI above or below 25 kg/m² over the range of 20–30 kg/m². Moreover, the results of the individual patient data meta-analysis may only be valid for patients with BMI values \leq 35 kg/m² as the study only included examinations with the standard M probe which has limited applicability in more obese patients [76•]. The XL probe has a greater depth of measurement below the skin surface and was introduced to reduce unsuccessful and unreliable liver stiffness measurements in more obese patients [77]. Although CAP measured using the XL probe tended to be higher than CAP measured using the M probe in the same patient, both probes appeared to have similar accuracy for the diagnosis of steatosis grades \geq S1, \geq S2, and S3 [58•]. Another study has shown that the 248-dB/m, 268-dB/m, and 280-dB/m recommended cutoffs for CAP for the diagnosis of steatosis grades \geq S1, \geq S2, and S3 may be used for the XL probe [67•]. On the other hand, a

study by Caussy et al. that used either the M probe or the XL probe based on the recommendation by the device suggested that the cutoff for CAP in detecting hepatic steatosis \geq 5% based on MRI-PDFF to be 288 dB/m [78].

The reliability criteria for CAP have not been defined. In a study using liver biopsy as the reference standard, the accuracy of CAP for the diagnosis of hepatic steatosis was significantly lower when the IQR was \geq 40 dB/m [63]. In another study using the MRI-PDFF as reference standard, CAP was found to be more accurate for the diagnosis of hepatic steatosis when the IQR was $<$ 30 dB/m [78]. Currently, CAP is considered reliable if the corresponding liver stiffness measurement is reliable. Liver stiffness measurement is considered reliable if the IQR/median is \leq 30%, or if the liver stiffness measurement is $<$ 7.1 kPa when the IQR/median is $>$ 30% [79•]. A study found that CAP declined after meal but returned to baseline after 150 min [80], while another study found no difference in CAP after meal [81]. As liver stiffness measurement has been shown to be affected by meal, transient elastography is usually performed after at least 2 h of fasting [82].

As transient elastography is noninvasive and easy to use, CAP has the potential to be used as a screening tool for fatty liver. Patients identified to have fatty liver should be given lifestyle advice and should undergo evaluation for other components of the metabolic syndrome, which should be treated accordingly if present, to reduce the risk of cardiovascular disease [83•]. Moreover, liver stiffness measurement that is available simultaneously with CAP allows identification of patients with more severe liver fibrosis who can then be referred to specialist doctors for further management. On the other hand, patients with chronic liver disease of various aetiologies undergoing liver stiffness measurement with FibroScan to evaluate for liver fibrosis can have evaluation for hepatic steatosis at the same time, which may be helpful in the overall management of the patient. For example, the presence of significant hepatic steatosis has been shown to be associated with more severe liver disease in patients with chronic hepatitis B infection [84], and CAP can prompt the attending doctor to manage the fatty liver and metabolic syndrome in these patients, when present. One of the limitations of CAP is that it does not have the ability for anatomical visualization, which is often required, for example in the investigation of abnormal liver tests or for hepatocellular carcinoma surveillance in patients with chronic hepatitis B. As mentioned before, CAP is impaired by increased body mass index and is less accurate to distinguish between the different grades of significant hepatic steatosis in obese patients. The MRI-PDFF has been shown to perform significantly better than CAP for distinguishing the different grades of significant hepatic steatosis in NAFLD patients [85•, 86•]. Another limitation of CAP is the lack of accuracy in following change in the degree of hepatic steatosis. A study that evaluated CAP for following change in hepatic steatosis determined by the MRI-

Table 2 Summary of studies that evaluated CAP for the diagnosis of steatosis grades using liver biopsy as reference standard since the summary by Chan et al. [58•]

Authors (year)	Study population	Mean BMI (kg per m ²)	Distribution of steatosis grades S0, S1, S2, and S3	AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and S3
Cardosa et al. 2015 [59]	136 patients with chronic hepatitis B	25	78%, 10%, 9%, and 3%	0.82, 0.82, and 0.97
de Ledinghen et al. 2016 [60]	261 NAFLD patients	30.2	0%, 29.9%, 38.3%, and 31.8%	The AUROC for diagnosis of steatosis grades \geq S2 and S3 was 0.80 and 0.66, respectively.
Chen et al. 2016 [61]	189 patients with chronic hepatitis B	22.5	51%, 27%, 16%, and 6%	0.88, 0.92, and 0.94
Hong et al. 2017 [62]	55 potential liver donors	23.6	34.5%, 54.5%, 11.0%, and 0%	The AUROC for diagnosis of steatosis grades \geq S1 and \geq S2 was 0.77 and 0.88, respectively.
Chan et al. 2017 [58•]	57 NAFLD patients; transient elastography was performed with both M and X probes.	30.2	29%, 17%, 35%, and 19%	The AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and S3 was 0.94, 0.80, and 0.69, respectively, using the M probe, and 0.97, 0.81, and 0.67, respectively, using the XL probe.
Xu et al. 2017 [75]	366 patients with chronic hepatitis B	23.4	62.6%, 33.9%, 2.2%, and 1.4%	0.78, 0.93, and 0.99
Wong et al. 2017 [63]	754 patients with chronic liver disease of various aetiologies; 46% had NAFLD.	27.2	29%, 33%, 19%, and 19%	The AUROC for diagnosis of steatosis grades \geq S1 was 0.88. In the derivation cohort, the AUROC for diagnosis of steatosis grades \geq S1 was 0.86, 0.89, and 0.76 in patients with IQR < 20 dB/m, 20–39 dB/m, and \geq 40 dB/m.
de Ledinghen et al. 2017 [64•]	236 patients with chronic liver disease of various aetiologies; 20.8% had NAFLD; transient elastography was performed with both M and XL probes.	24.4	51.7%, 22.5%, 10.2%, and 15.7%	In the validation cohort, the AUROC for diagnosis of steatosis grades \geq S1 was 0.90 and 0.77 in patients with IQR < 40 dB/m and \geq 40 dB/m
Andrade et al. 2017 [65]	159 patients with chronic liver disease of various aetiologies; 42.1% had NAFLD.	1.9% had BMI < 18.5 kg per m ² , 50.3% had BMI 18.5–24.9 kg per m ² , 30.8% had BMI 25.0–29.9 kg per m ² , and 17.0% had BMI > 30 kg per m ²	18.9%, 32.7%, 22.6%, and 25.8%	The AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and S3 was 0.82, 0.83, and 0.89, respectively, using the M probe, and 0.88, 0.92, and 0.93, respectively, using the XL probe.
Thiele et al. 2018 [66]	269 patients with alcohol overuse	26	28%, 35%, 24%, and 13%	0.77, 0.78, and 0.88
Chan et al. 2018 [67•]	180 patients with chronic liver disease of various aetiologies:	29.5	9.4%, 28.3%, 43.9%, and 18.3%	The AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and

Table 2 (continued)

Authors (year)	Study population	Mean BMI (kg per m ²)	Distribution of steatosis grades S0, S1, S2, and S3	AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and S3
	86.7% had NAFLD; transient elastography was performed with both M and XL probes.			S3 was 0.84, 0.76, and 0.61, respectively, using the M probe, and 0.91, 0.78, and 0.65, respectively, using the XL probe. The AUROC for diagnosis of steatosis grades \geq S1 was 0.94.
Mendes et al. 2018 [68]	312 patients with chronic hepatitis C infection; steatosis grade was based on digital morphometric quantification of liver biopsy slides.	27.2	19.2%, 28.5%, 31.1%, and 21.2%	
Yen et al. 2018 [69]	54 liver donors	24.0	47 subjects had no hepatic steatosis while the remaining 7 subjects had hepatic steatosis ranging from 10 to 30%.	The AUROC for diagnosis of steatosis grade \geq S1 was 0.96.
Eddowes et al. 2019 [70]	404 consecutive adults who underwent liver biopsy for suspected NAFLD	33.8	12%, 23%, 28%, and 36%.	0.87, 0.77, and 0.70
Rout G et al. 2019 [71]	462 patients with chronic liver disease of various aetiologies; 19.3% had NAFLD	23.4	71.6%, 16.0%, 8.4%, and 3.9%	0.88, 0.89, and 0.88
Baumeler et al. 2019 [72]	224 patients with chronic liver disease of various aetiologies; 23.2% had NAFLD.	26.8	37.9%, 36.6%, 14.7%, and 10.7%	0.78, 0.83, and 0.82
Somda et al. 2019 [73]	249 morbidly obese patients who underwent sleeve gastrectomy; in cases with probe-to-capsule distance > 35 mm, CAP was adapted for a deeper measurement.	43.8	15.7%, 26.1%, 20.5%, and 37.7%	CAP was not performed at a sufficient depth in 130 patients, and the adapted CAP was significantly lower than the standard CAP. After adapting CAP in patients with probe-to-capsule distance > 35 mm, the AUROC for diagnosis of steatosis grades \geq S1, \geq S2, and S3 was 0.86, 0.83, and 0.79, respectively.
Semmler et al. 2019 [74]	88 patients with advanced chronic liver disease and/or portal hypertension defined by liver stiffness measurement \geq 10 kPa and/or hepatic venous pressure gradient (HVPG) \geq 6 mmHg who underwent liver biopsy, CAP, and HVPG.	25.4	53.4%, 31.8%, 12.5%, and 2.3%	AUROC for diagnosis of steatosis grades \geq S1 was 0.69 in the overall study population, 0.83 in patients with HVPG < 10 mmHg, and 0.63 in patients with HVPG \geq 10 mmHg.

PDFF found that the accuracy was 87.5% when the change in CAP was > 38 dB/m, but the accuracy was only 29.3% when the change in CAP was < 38 dB/m. The prognostic value of CAP is currently unclear. One study found CAP to be predictive of clinical decompensation and bacterial infections independent of liver stiffness measurement in patients with compensated advanced chronic liver disease [87], while another study found CAP to be not predictive of first and further hepatic decompensation among patients with compensated advanced chronic liver disease [88]. In a prospective study on 4282 patients with reliable baseline transient elastography, CAP did not predict liver-related event, cancer, or cardiovascular event [89]. Further studies on the prognostic value of CAP is awaited.

Histopathological Examination of Liver Biopsy Specimen

Nonalcoholic steatohepatitis (NASH) is defined histologically by the presence of significant hepatic steatosis, lobular inflammation, and hepatocyte ballooning with or without fibrosis. Currently, the diagnosis of NASH can only be reliably made by histopathological examination of a liver biopsy specimen [90•]. The NASH Clinical Research Network has introduced a scoring system for a standardized approach towards the reporting of histopathological findings of liver biopsy of NAFLD patients [91••]. The grading for hepatic steatosis is S0 for < 5%, S1 for 5–33%, S2 for 33–66%, and S3 for > 66%. However, the grading is subjective to the observer's estimation and may suffer from intra- and inter-observer variability. Moreover, the semi-quantitative nature of the grading means that a large degree of change in hepatic steatosis is required for a change in grade. This means that it will not be able to detect small changes in hepatic steatosis following intervention. Liver biopsy may also be limited by sampling variability, although a study on patients with two liver biopsies taken at different angles did show substantial agreement for grading of steatosis [92]. These factors challenge the role of liver biopsy in the assessment of hepatic steatosis as the procedure is also invasive and associated with a small risk of serious complications. Moreover, several other noninvasive methods are available for the diagnosis of hepatic steatosis, from the simple and widely available ultrasonography to the more sophisticated transient elastography that come with simultaneous assessment of steatosis and fibrosis, and the highly accurate MRI-based methods. Nevertheless, a liver biopsy is still essential for the diagnosis of NASH, which has important prognostic value, is recommended prior to the use of certain medications such as vitamin E and pioglitazone, and is often required prior to enrolment in clinical trial, although this may change when safer and more effective drugs

addressing the many faces of metabolic syndrome become available in the future.

Enhancement of Histopathological Grading of Hepatic Steatosis

Stereological analysis using grid-point counting method combined with the Delesse principle has been shown to have superior conformity and repeatability for the measurement of hepatic steatosis on liver biopsy specimens compared with histopathologist grading. For example, the intraclass coefficient for assessment of hepatic steatosis by three experienced liver pathologists in a study on 59 liver biopsy specimens was 0.79 with a repeatability coefficient of 38%, whereas the intraclass coefficient for stereological measurement of hepatic steatosis by three analysts was 0.86 with a repeatability coefficient of 8% [93•]. However, stereological analysis is time-consuming when performed manually and is not practical outside of research setting. The development of computer-assisted stereology system may improve the uptake of this method for measurement of hepatic steatosis in the future. Second harmonic generation microscopy is an automated novel optical imaging modality that can potentially identify and assess clinically pertinent aspects of liver histology [94]. A laser is passed through a pulse compressor and an acoustic-optic modulator, before being routed by a dichroic mirror through an objective lens to the liver biopsy sample, where two photon-excited fluorescence emissions and second harmonic generation signal are collected and processed for detection. Specific aspects of liver histology can be measured using dedicated algorithms. The technology has been shown to provide reliable and reproducible measurements of fibrosis in liver biopsy specimen previously [95], and steatosis more recently [96•, 97•]. In a study on 86 liver biopsy specimens, very strong correlation was observed in the assessment of hepatic steatosis by histopathologists and second harmonic generation microscopy with Pearson correlation of 0.93. In a subsequent study on 329 liver biopsy specimens incorporating second harmonic generation-based tool for quantification of fibrosis, inflammation, hepatocyte ballooning, and steatosis, a very strong correlation was similarly observed for steatosis with Pearson correlation of 0.88. The correlation was strong for lobular inflammation and fibrosis but only moderate for hepatocyte ballooning [94]. This technology appears promising in overcoming observer variability and providing more precise quantification of the different histological components of NAFLD but requires further refining and validation. However, a dedicated machine is required for image acquisition and the analysis is performed using proprietary algorithms, which may hamper its uptake for wider use.

Conclusion

Quantification of hepatic steatosis is important, especially in clinical trials and for follow-up of NAFLD patients on lifestyle intervention or medical therapy. Although liver biopsy is regarded as the gold standard, its use is limited by the invasive nature of the procedure and the availability of noninvasive tests such as US, MRI-PDFF, and CAP. A good understanding of the advantages and disadvantages of each of these modalities will help one choose the most suitable method for quantifying hepatic steatosis in NAFLD patients in clinical trials as well as in day-to-day clinical practice.

Compliance with Ethical Standards

Conflict of Interest Kee-Huat Chuah declares no potential conflicts of interest.

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Human and Animal Rights and Informed Consent This article does not contain any studies with human or animal subjects performed by any of the authors.

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- Of importance
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